

# Optimal Control by Transmit Frequency in Tissue Harmonic Imaging

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Tours, France



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**Inserm**

Institut national  
de la santé et de la recherche médicale

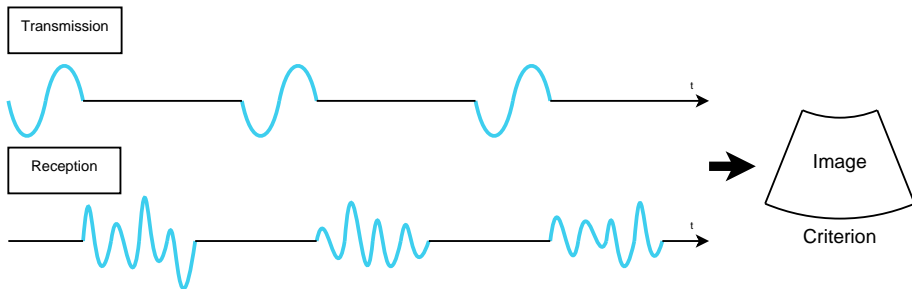
# Outline

- 1 Introduction
  - Ultrasound Imaging System
  - Ultrasound Second Harmonic Imaging
  - Problematic
- 2 Implementation of the Closed Loop System
  - Cost Function
  - Algorithm
- 3 Materials
- 4 Results
  - Simulation
  - Experiment
- 5 Conclusions & Prospects

# Introduction

## Ultrasound Imaging System

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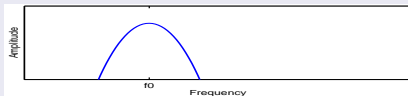


## Ultrasound Imaging System

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## Transmission



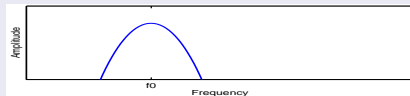
## Reception

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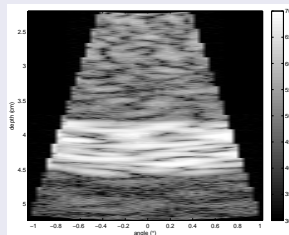
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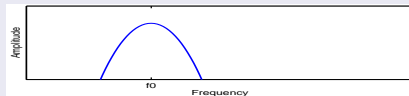
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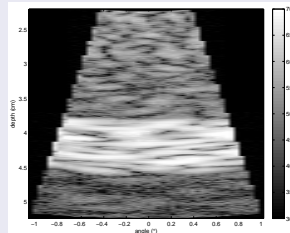
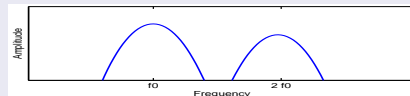
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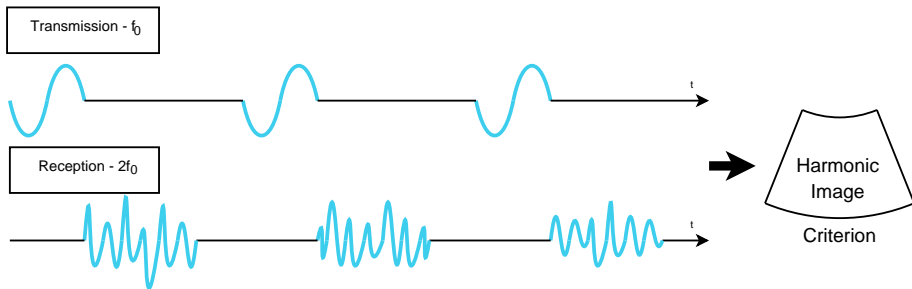
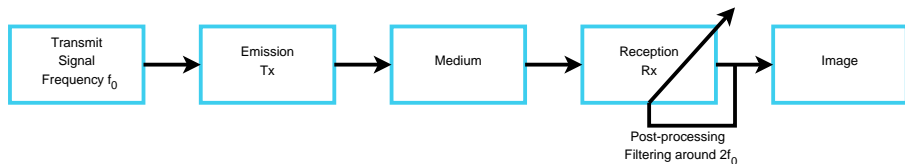
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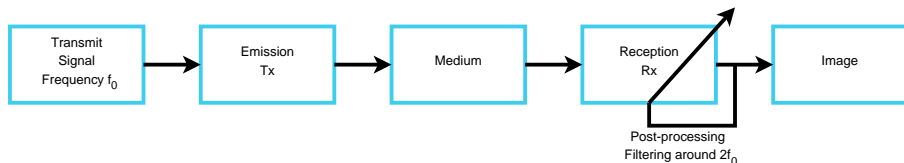


# Ultrasound Second Harmonic Imaging

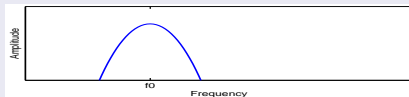




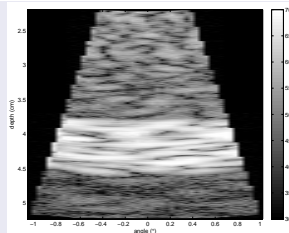
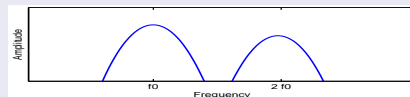
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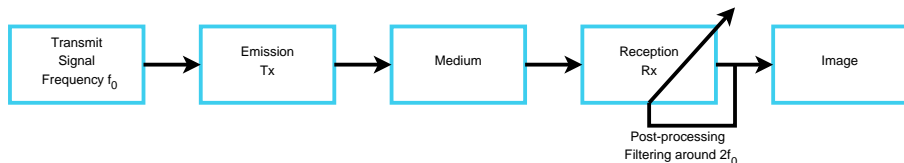
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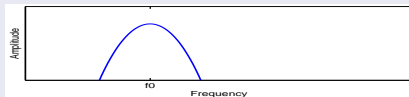
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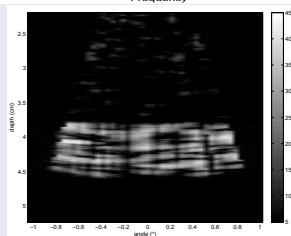
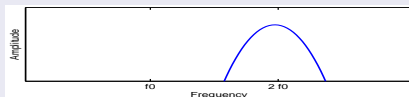
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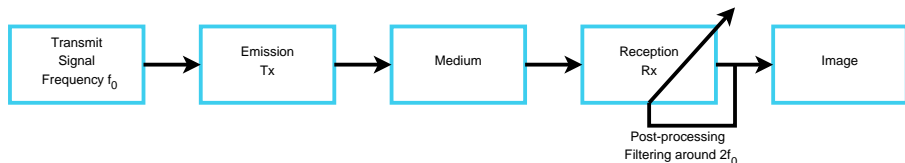
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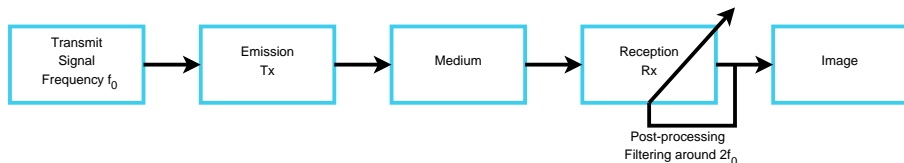
# What is the best frequency ?



## How to choose the transmit frequency $f_0$ ?

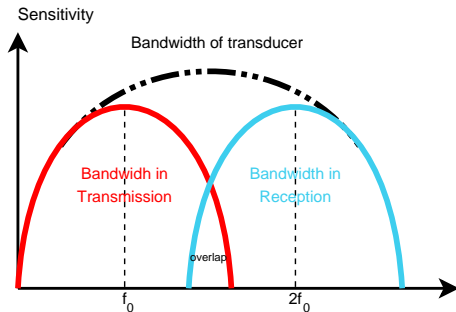
- Advice :  $2/3f_c$  with  $f_c =$  central frequency of the transducer
- Is it optimal ?

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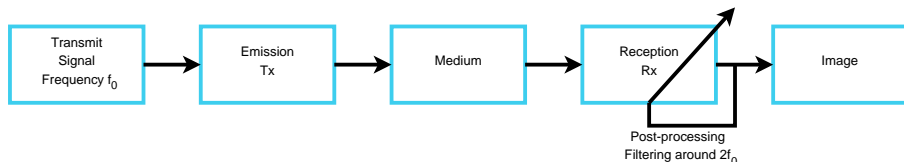


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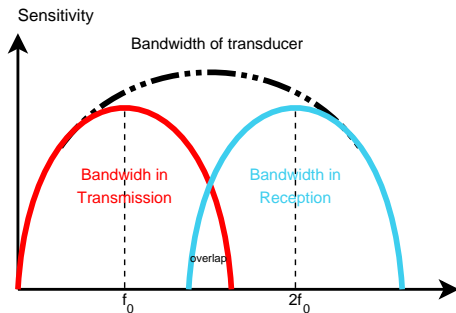


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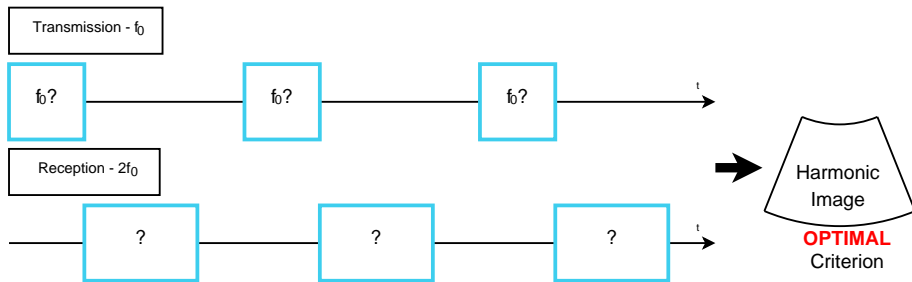
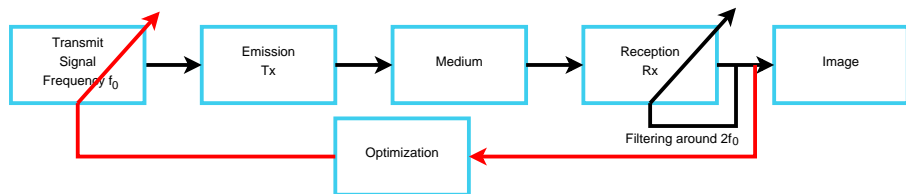


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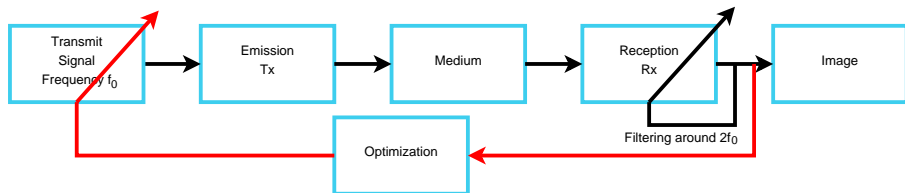


# Optimal Transmit Frequency for Ultrasound Imaging System



## Implementation of the Closed Loop System

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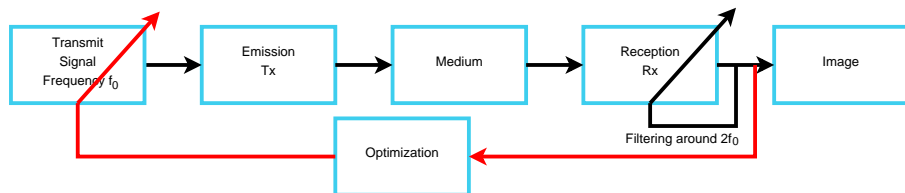


## Setting of Iterative Optimization

- 1 Choice of the Cost Function  $J(\theta)$
- 2 Choice of the parameters  $\theta$
- 3 Choice of the optimization algorithm



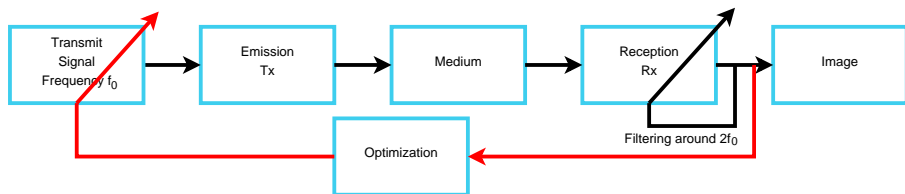
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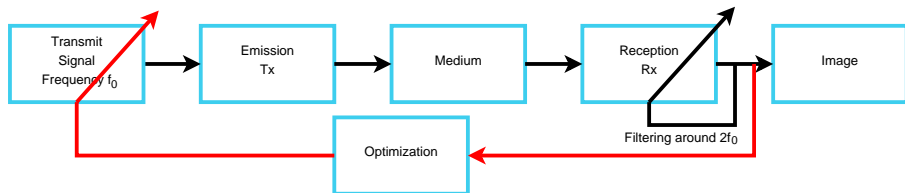
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## Setting of Iterative Optimization

- 1 Choice of the Cost Function  $J(\theta)$
- 2 Choice of the parameters  $\theta \rightarrow$  **Transmit frequency  $f_0$**
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# Find the Cost Function for the Goal

## Goal

Maximize the contrast by the transmit frequency  $f_0$

### ① Choice of the Cost Function

- Maximize nonlinear behavior
- Minimize linear behavior
- Cost Function "*Contrast Harmonic to Fundamental Ratio*" :

$$CHFR(f_0) = \frac{\text{Second Harmonic Power}}{\text{Fundamental Power}}$$

- Constraint : constant transmitted power

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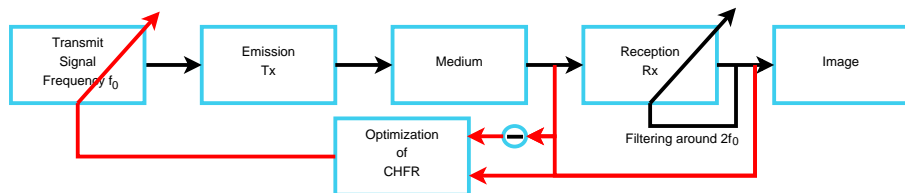
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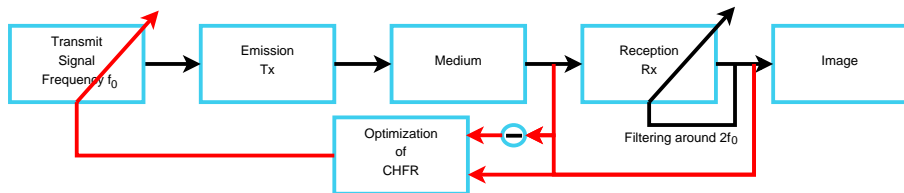


## Algorithm

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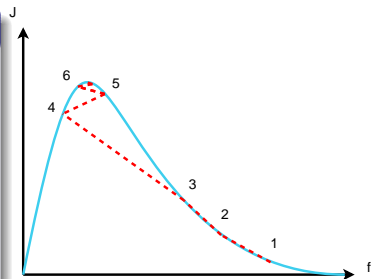


## ③ Algorithm and Principle

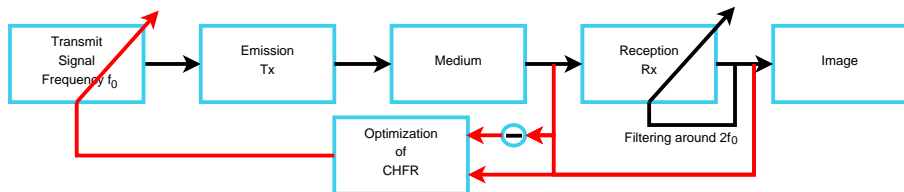
### • Method of Gradient

- Seek the maximum by “going up the descent”

$$f_{k+1} = f_k + \alpha_k \cdot \nabla CHFR(f_k)$$



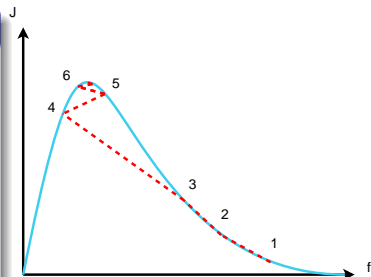
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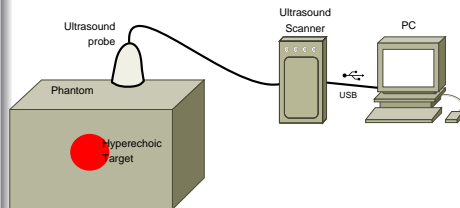


# Materials

# Simulation and Experimental Setup

## Experiment

- “Open” Ultrasound Scanner  
(MultiX WM, M2M, Les Ulis, France)
- Probe centred at  $f_c = 4$  MHz  
(Vernon SA, Tours, France)
- Phantom with hyperechoic target  
(CIRS, Norfolk, VA, USA)



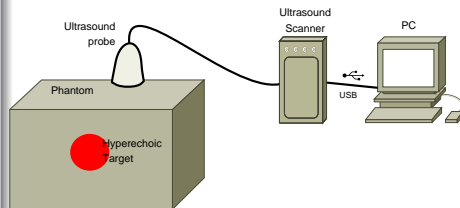
## Simulation

- Transducer centred at  $f_c = 3.5$  MHz
- Nonlinear propagation: pseudo-spectral method [Anderson, 2000]
- Tissue with a blood vessel

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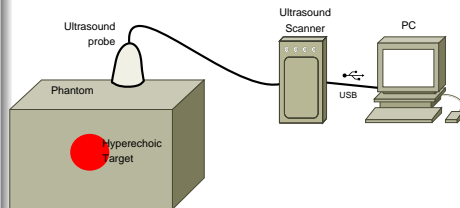
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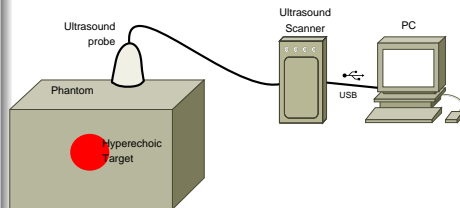
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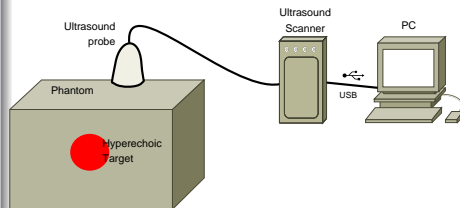
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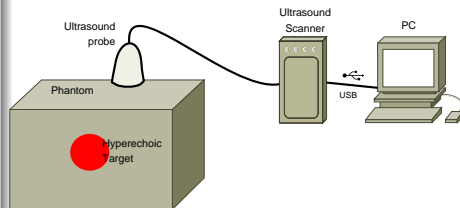
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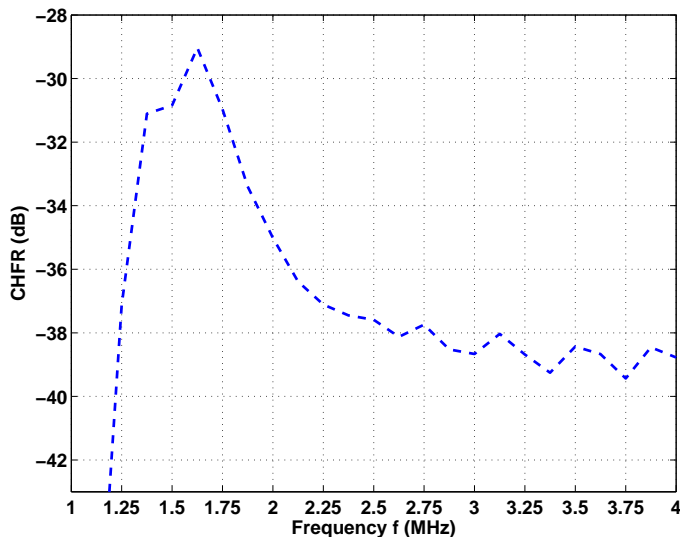


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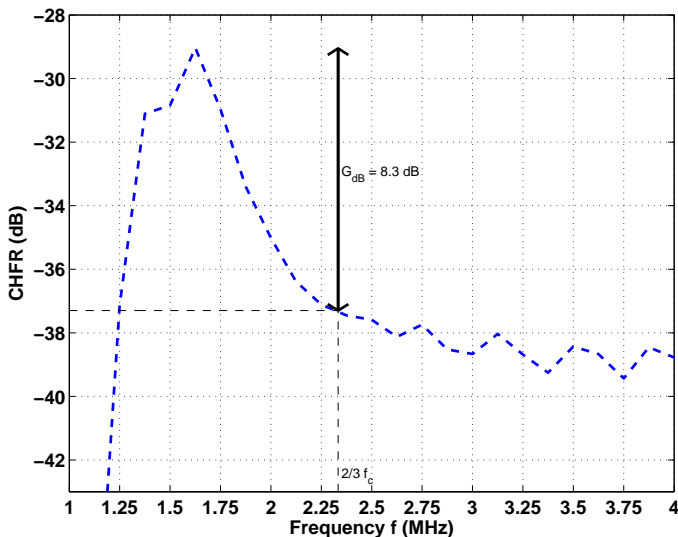
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# Results

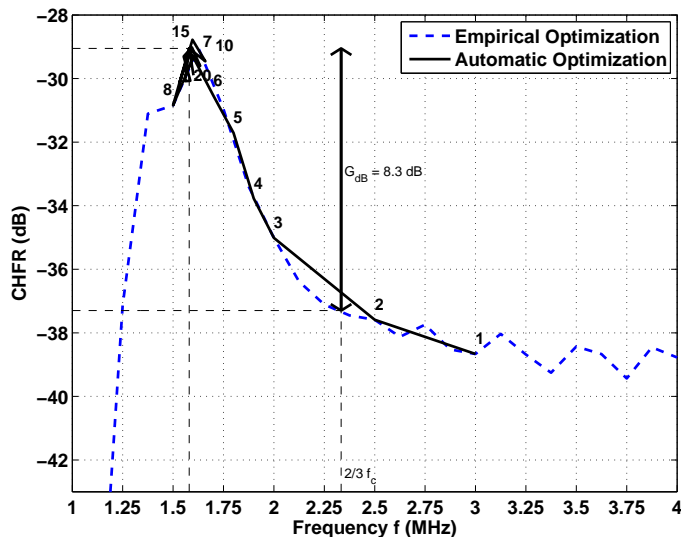
# Simulation: Empirical Optimization



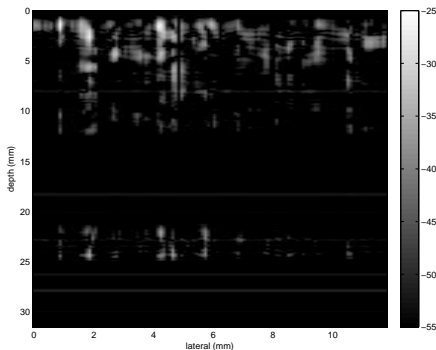
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# Simulation: Automatic Optimization

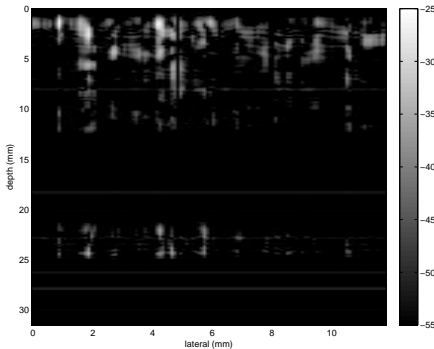


# Simulation: Synthetic Images

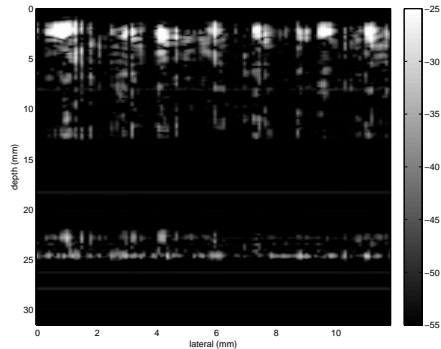


$$f_0 = 2/3f_c = 2,3 \text{ MHz}$$

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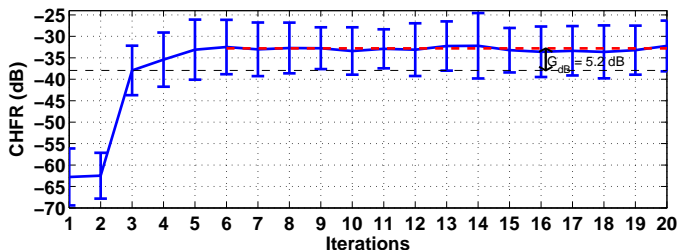
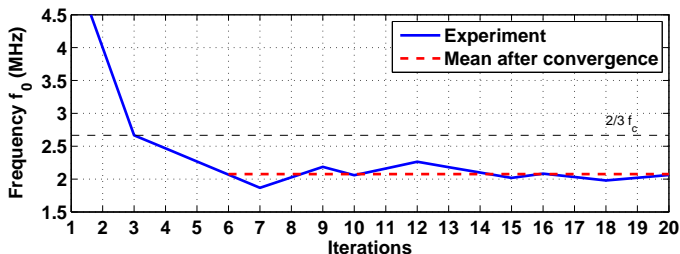
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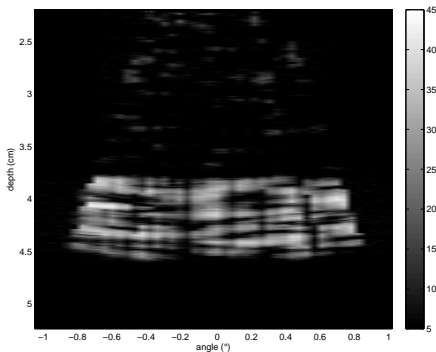
$$f_0 = f_{0,opt} = 1,6 \text{ MHz}$$



# Experiment: Automatic Optimization

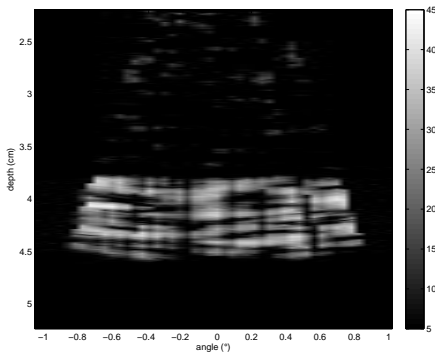


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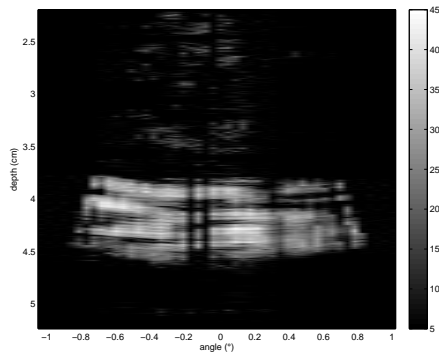


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## Conclusion & Prospects

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- Automatic optimization of the contrast (*CHFR*)
  - Adapt itself to optimize the contrast
  - Setting without knowlegde of medium or transducer
  - Gain of around 5 dB with our closed-loop system
  - Prospects: application to another harmonic imaging methods

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# Thank you for your attention

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jean-marc.girault@univ-tours.fr



Institut national  
de la santé et de la recherche médicale